

# ***In vivo* optical imaging : revealing endogeneous optical contrast at depth**



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# Why using optical imaging *in vivo* ?

- ✓ Near infra-red light penetrates into tissue

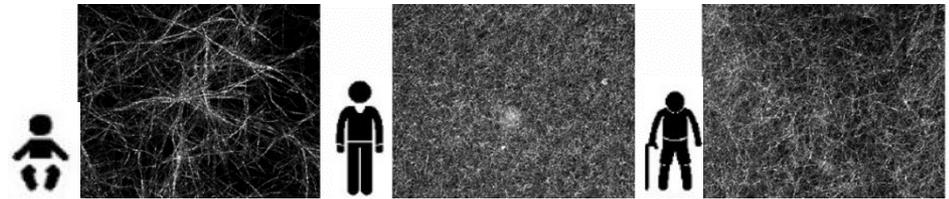


- ✓ Interactions between light and tissue through:

Absorption



Scattering : micro-structure



Collagen structure at different stage of life

- ✓ Spectral information can discriminate tissue components



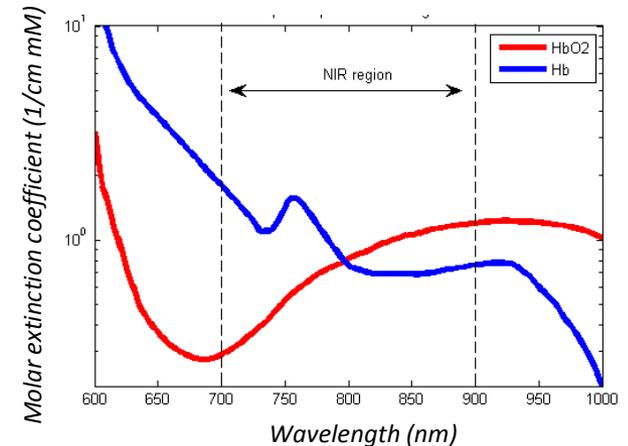
Hemoglobin, melanin, lipid, water ...

➔ bring **anatomical**, **functional** and **molecular** information

# Information provided by optical properties *in vivo*

## Absorption:

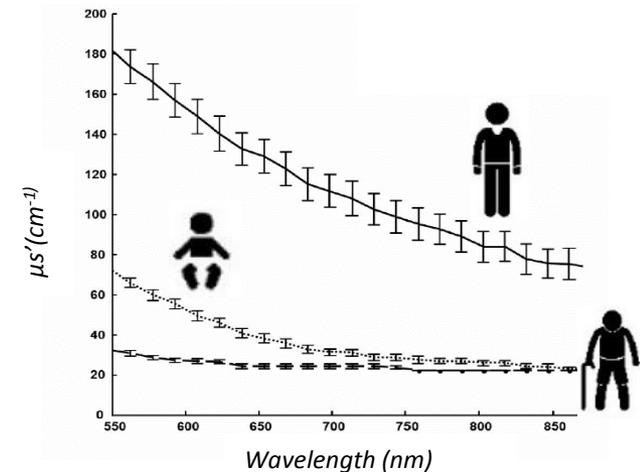
- **Hemodynamic parameter** (Oxy/Deoxy Hemoglobin, SO<sub>2</sub>, blood volume,...)
- **Chromophores concentrations** (Hemoglobin, Melanin, Water, Lipid, ...)



## Scattering :

- **Tissue structure** (muscle, fat, tumoral structure, collagen modification..)

➔ **Application:** Monitoring in space and time for diagnostic or observation



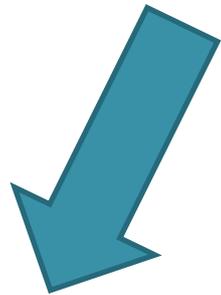
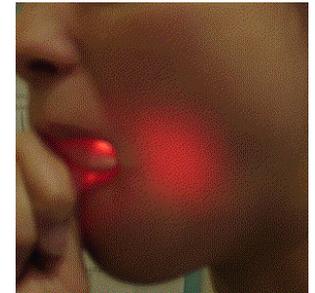
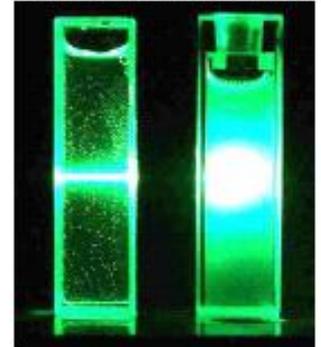
# Optical imaging and Photoacoustic imaging

Light/tissue interactions contain **anatomical**, **functional** and **molecular** information

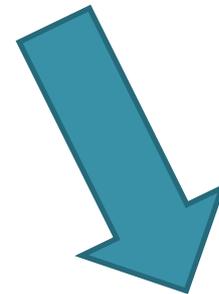
**BUT**

- Can we **achieve imaging of endogenous optical contrast at depth** in strongly scattering tissues ?
- Can we **separate absorption from scattering** ?

clear medium    turbid medium



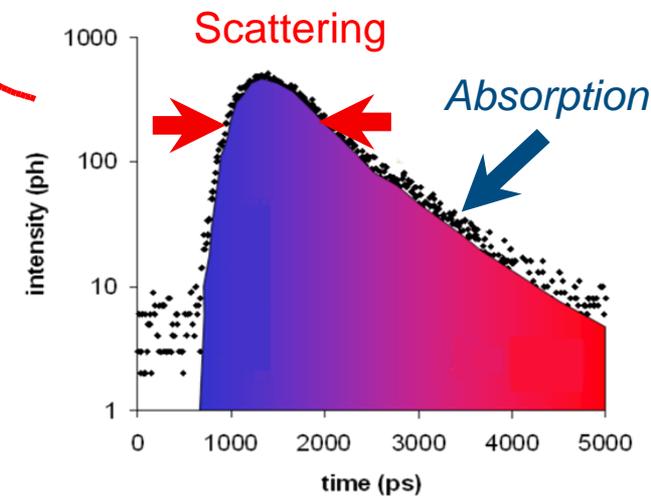
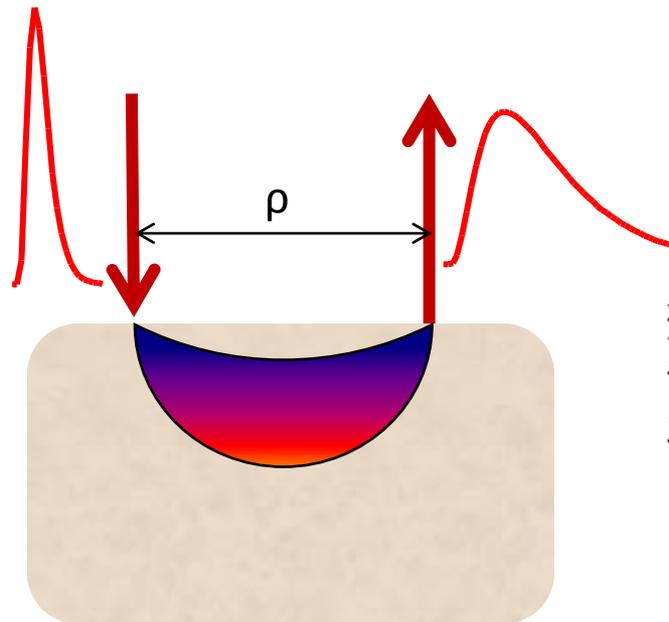
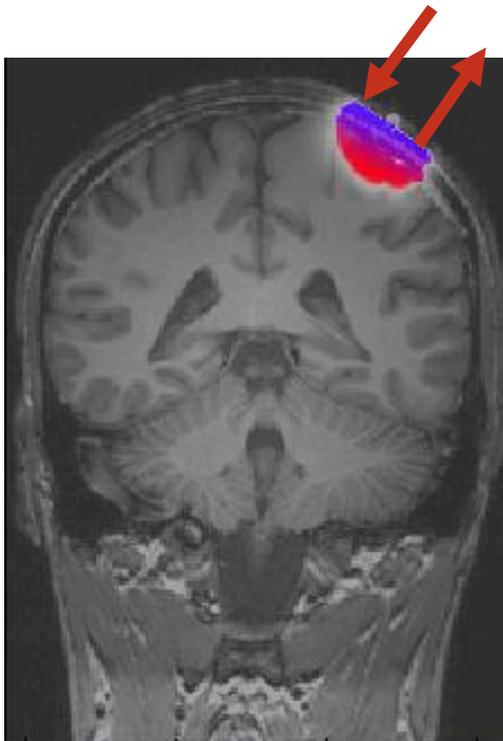
✓ Diffuse optics



✓ Photoacoustics

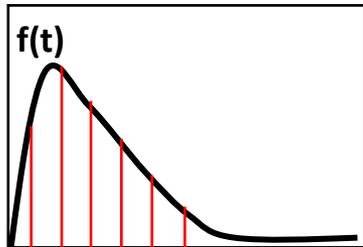
# Endogenous Optical imaging – Time-resolved approach

- **Why time-resolved measurements?**
  - separation of effects due to scattering from those due to absorption
  - «time encodes depth»

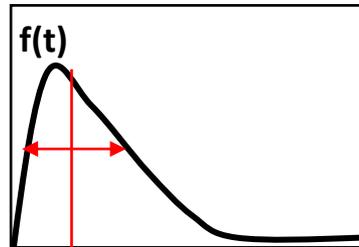


# Optical Imaging : Principle

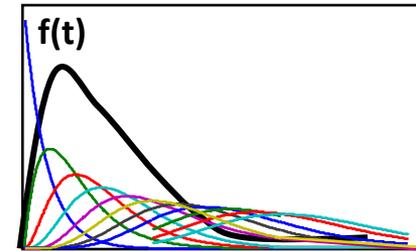
## Time-selection of detected photons



*Temporal sampling*

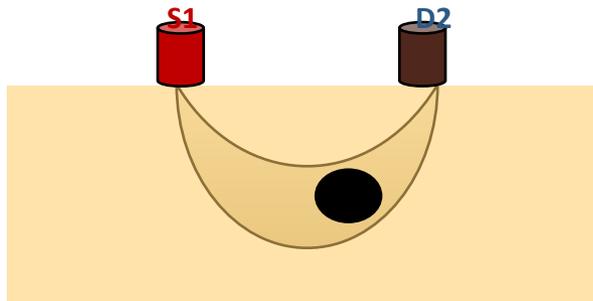


*Temporal moment*

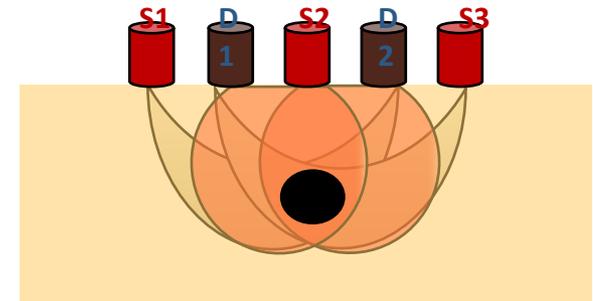


*Temporal window*

## Acquisition protocol



*Time-resolved - Diffuse optical Spectroscopy  
TR-DOS*



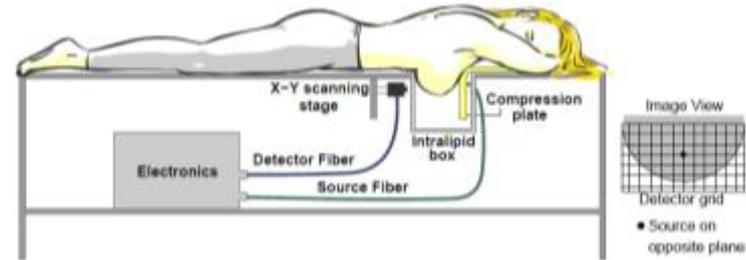
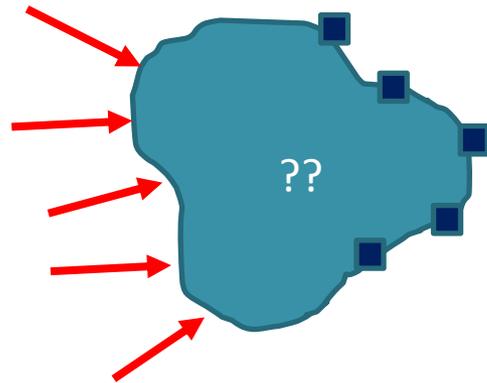
*Time-Resolved - Diffuse Optical Tomography  
TR-DOT*

➤ **Absolute quantification of absorption and diffusion**

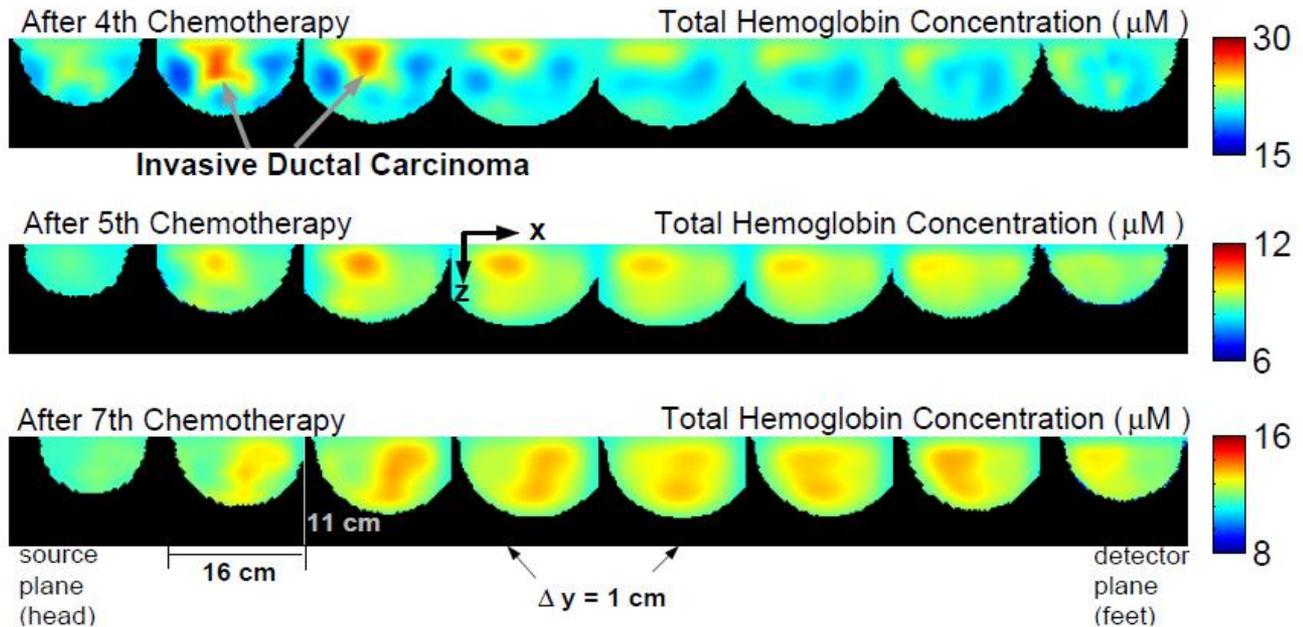
# Optical Imaging : Principle

## ■ Time-Resolved Optical Diffuse Tomography: TR-DOT

A.G. Yodh J Biomed Opt. 2009 Mar-Apr;14(2):024020: 1-18.



- ?? Unkown Optical properties
- Detection point
- Excitation point



# Optical Imaging : Technical implementations

- Time-resolved instrumentation



- Frequency-Domain instrumentation

Instrumentation complexity

Level of information per source-detector pair

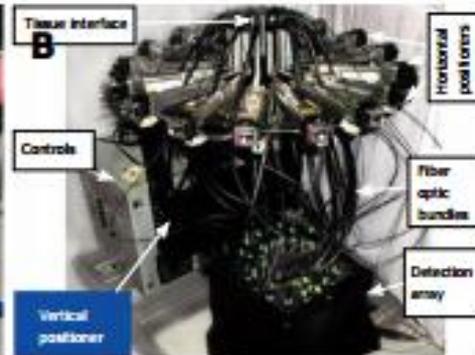
TD > FD

TD > FD

- Different acquisition geometries



**FD - DOT**  
*Parallel Plate*



**FD - DOT**  
*Ring-Type*



**FD - DOT**  
*Hand-Held*



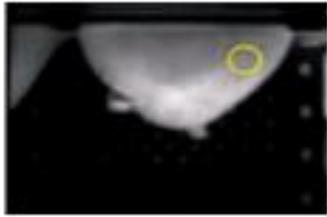
**TR-DOT**  
*Transmission type*

# Optical Imaging : Applications

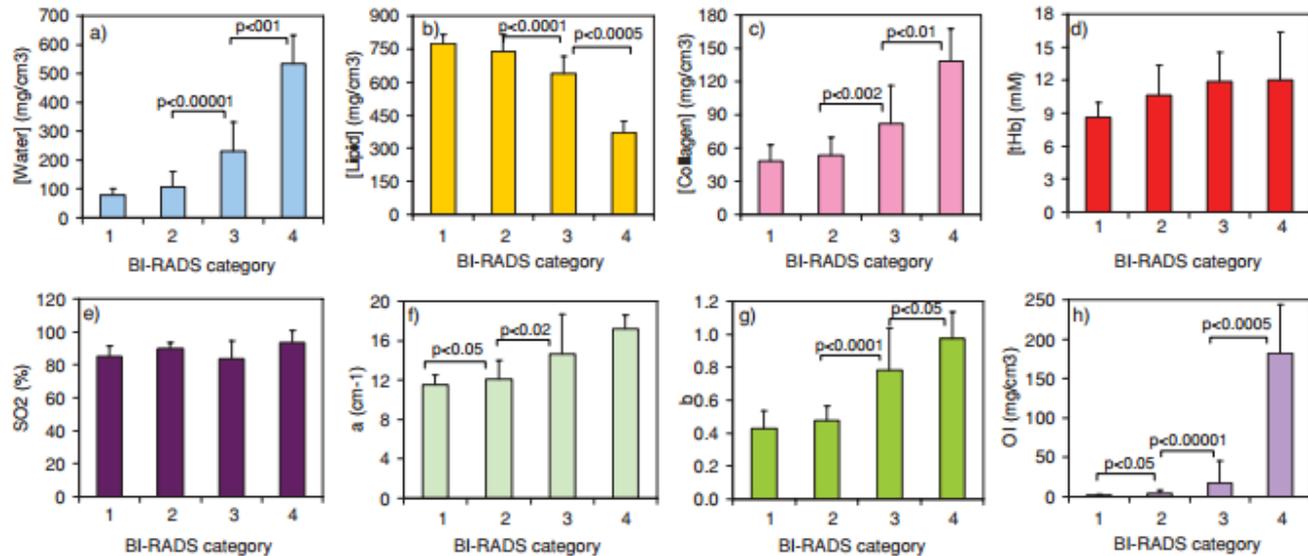
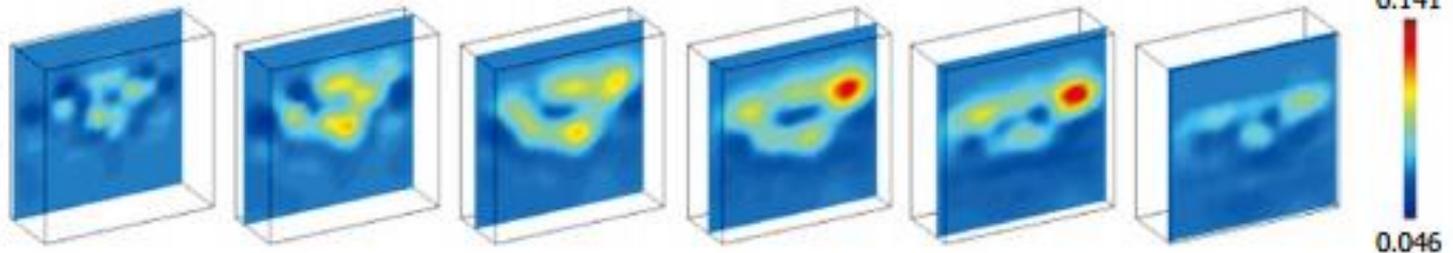
## Mammography

K. Lee. World J Clin Oncol. 2011 Jan 10; 2(1): 64–72.

**B**



*malignant tumor*

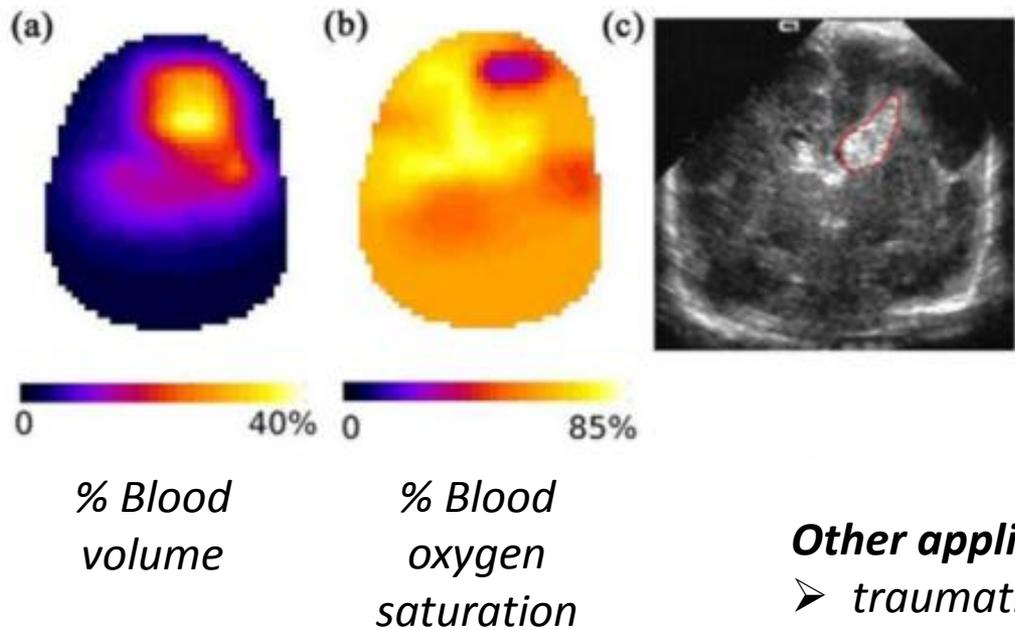


P. Taroni. JBO, 2010, 15(6)

# Optical Imaging : Applications

## Brain: Example of neonates

Hebden JC. *European Radiology* 2007 17(11):2926–2933



L. Dempsey Proc. SPIE 953818, ECBO (July 16, 2015)



TR-DOT

Whole-head functional brain imaging of neonates at cot-side using time-resolved diffuse optical tomography

### **Other application in BRAIN**

- *traumatic brain injury (TBI)*
- *subarachnoid hemorrhage (SAH)*
- *ischemic stroke*
- *sleep apnea and other sleep disorders*
- *intraoperative brain monitoring*

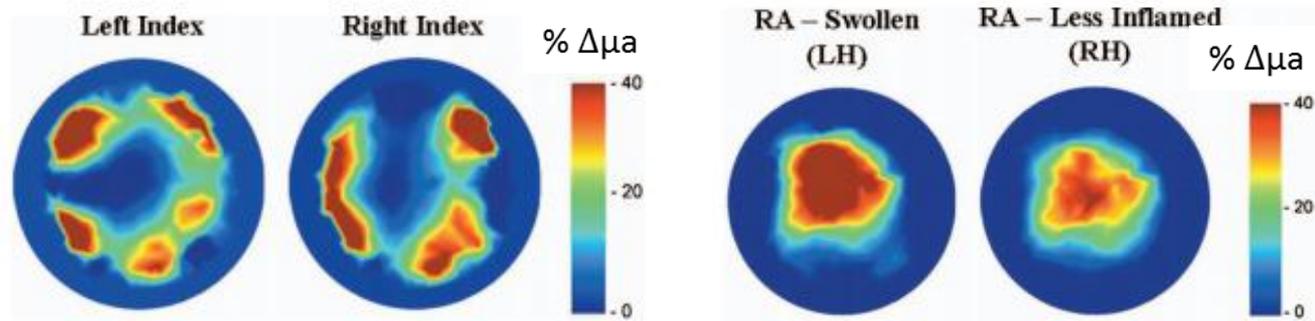
# Optical Imaging : Applications

## Other applications: Functional responses

- Tomography of finger joint physiology and disease

*M.Lasker. JBO 2015, 12(5)*

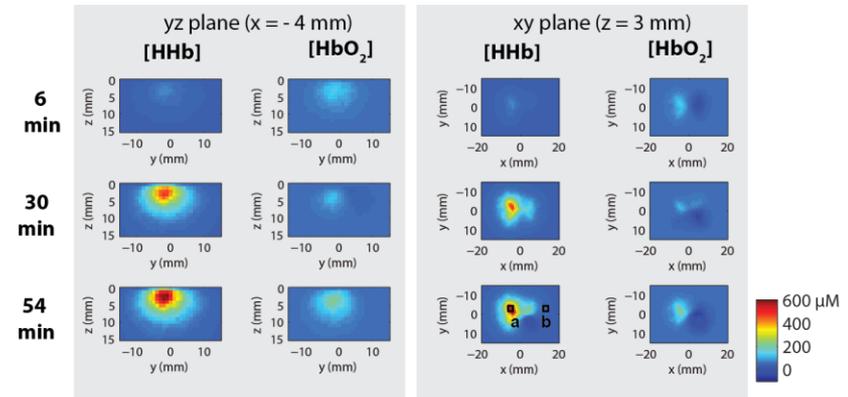
CW-DOT



- Flaps monitoring

*L. DiSieno Proc. SPIE 9538, ECBO (July 16, 2015)*

FD-DOT  
➔ Depth

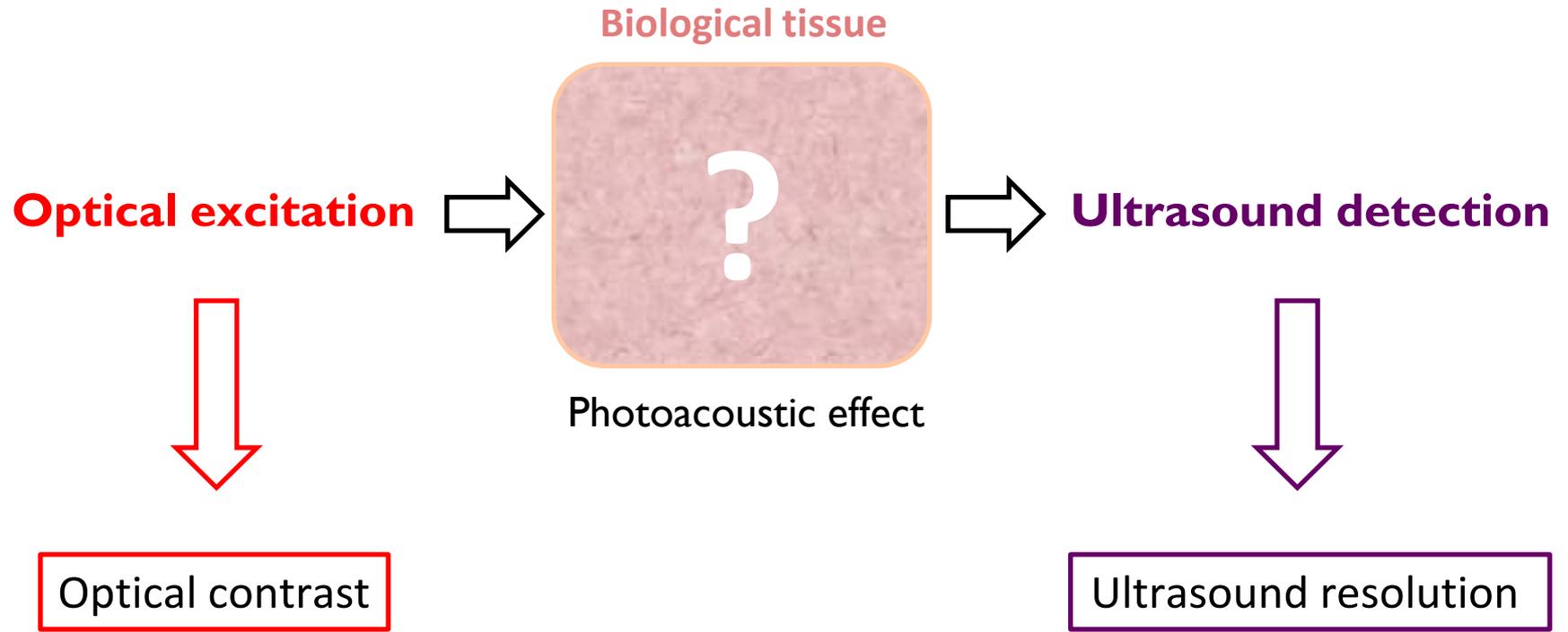


- Liebert / Hebden/etc...

# Synthesis

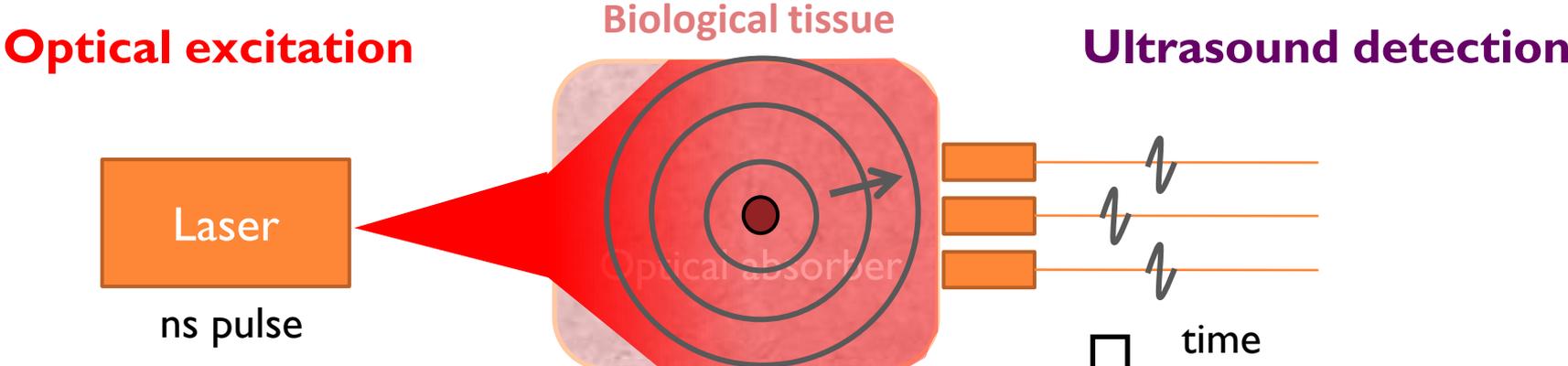
	Diffuse optics TR-DOT	Photoacoustics
Image contrast	Absorption and scattering	
Spatial resolution	From ~ mm at surface to ~ cm in depth <i>depending on the number of source/detector pairs, depth and <math>(\mu_a, \mu_s')</math></i>	
Penetration depth	~ 2.5 cm more in case of diffusing medium (breast)	
Temporal resolution	From ~s (spectroscopy) to ~min (optical fibers helmet) <i>depending on the number of source/detector pairs, depth and <math>(\mu_a, \mu_s')</math></i>	
Accessible organs	All externally or endoscopy Brain + monitoring	
Typical contrast agents	Indocyanine green	

# Photoacoustic imaging: a multiwave modality



Spatial resolution : < 1 mm at cm-depth

# Photoacoustic imaging : principle



Photoacoustic effect :  
Optical absorption of **scattered light**  
+ thermo-elastic expansion

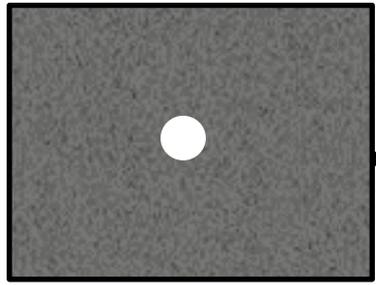
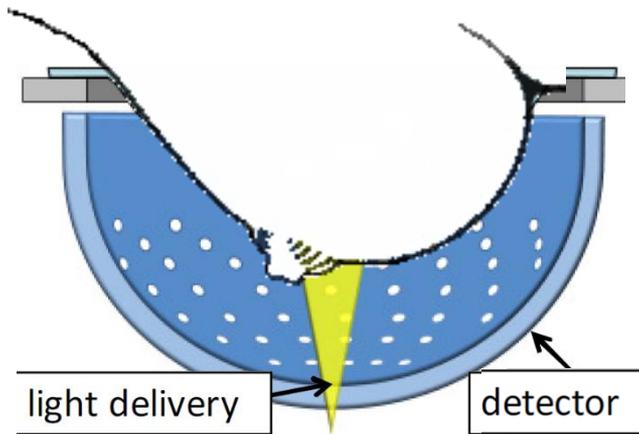


Image formation

Ratio penetration depth / resolution ~ 200

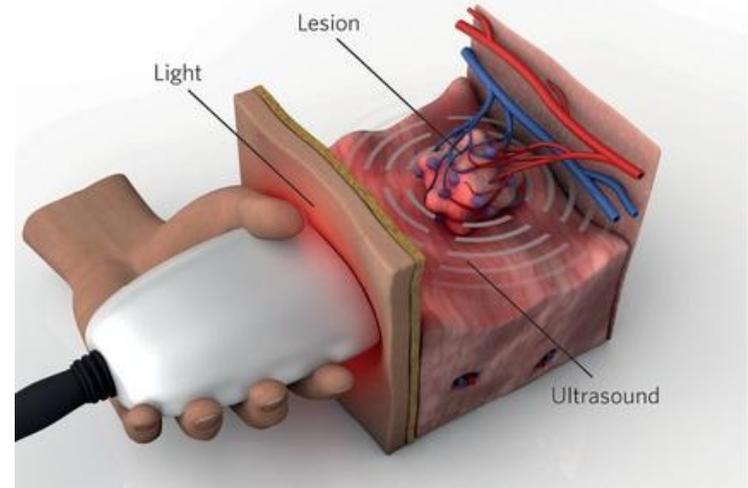
# Photoacoustic imaging : Technical implementations

## Tomographic detection



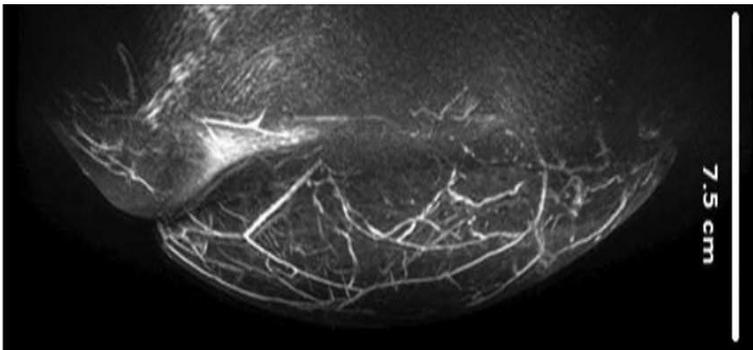
Optosonics Inc., Endra Inc.

## Hand-held detector array



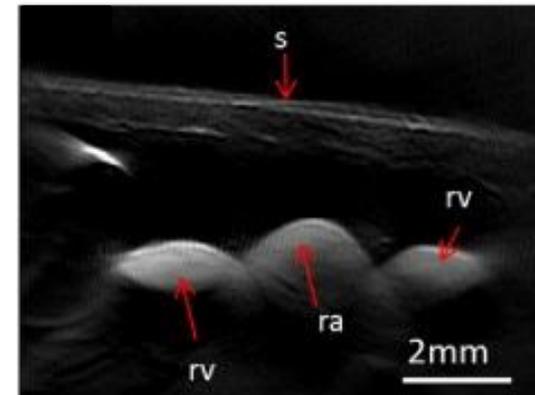
Taruttis A. and Ntziachristos V., Nat. Photo. 9, 2015

## Human breast



Kruger R. et al, Med. Phys. 40 (11), 2013

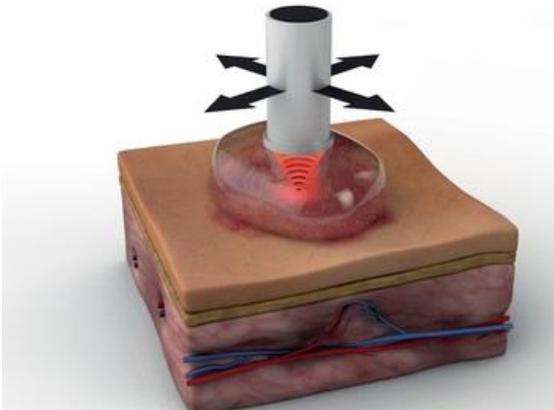
## Human wrist



Buehler R. et al, Opt. Lett. 38 (9), 2013

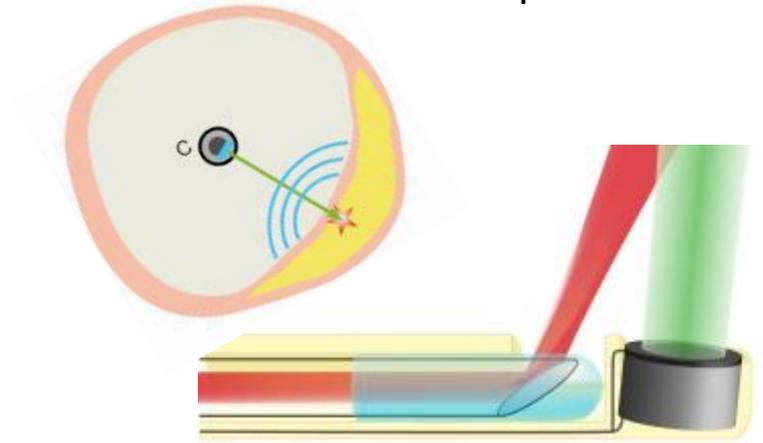
# Photoacoustic imaging : Technical implementations

Scanning mode

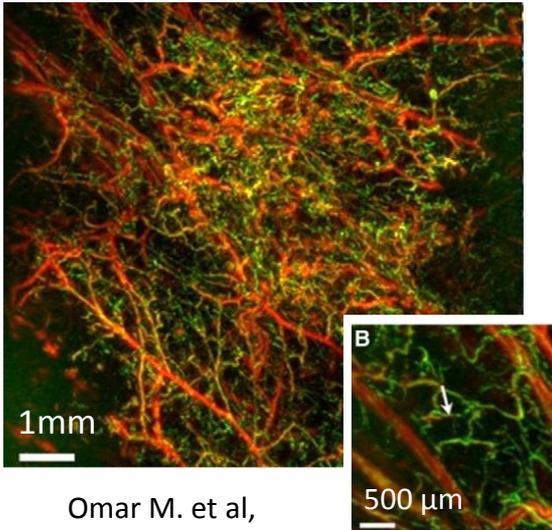


Taruttis A. and Ntziachristos V., Nat. Photo. 9, 2015

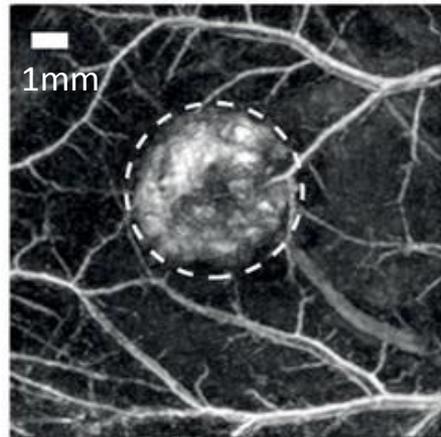
Endoscope



Sub-cutaneous tumors

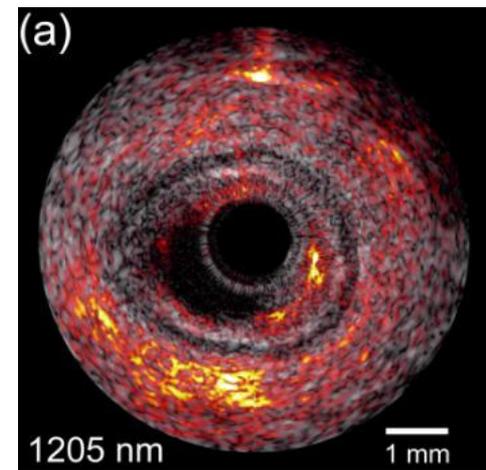


Omar M. et al, Neoplasia, 7, 2015



Laufer et al, J. Bio. Opt., 17(5), 2012

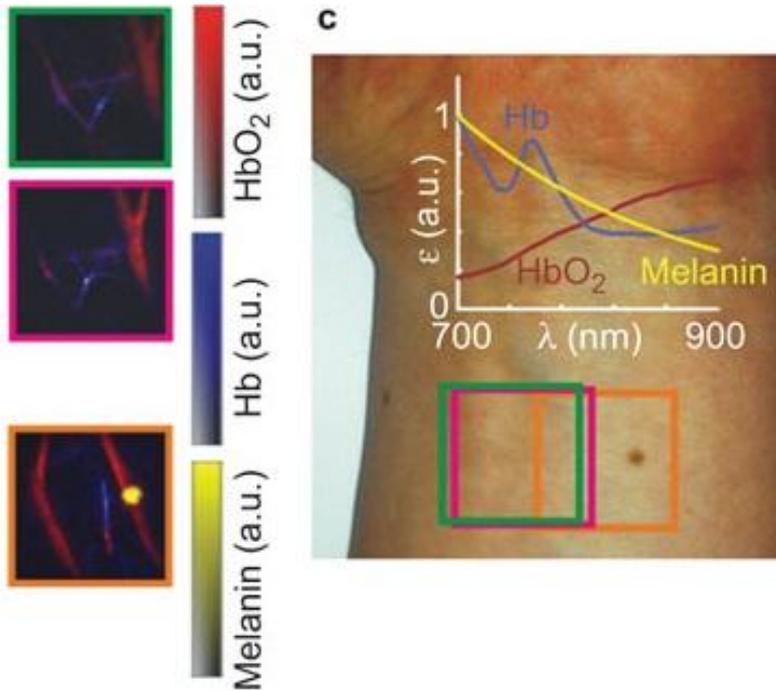
Coronary artery with plaque



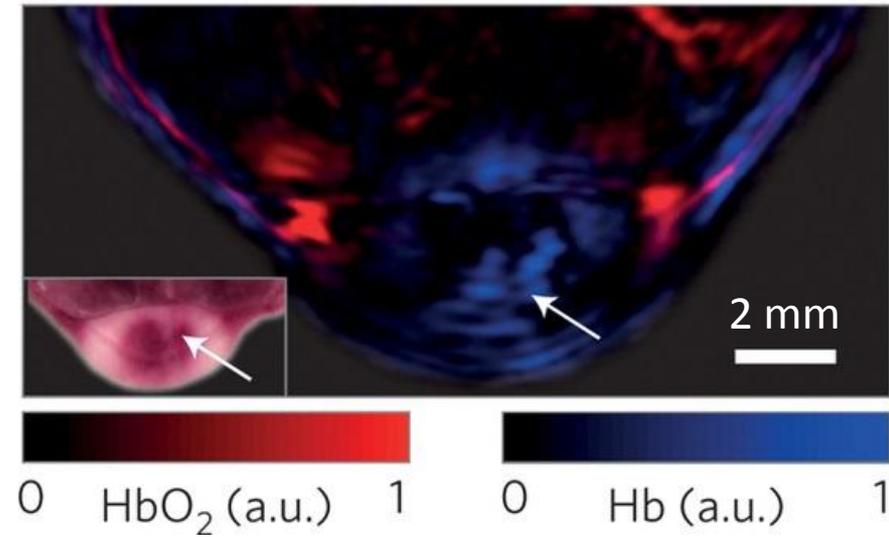
Jansen K. et al, Opt. Exp., 21 (18), 2013

# Photoacoustic imaging : blood oxygenation

Human wrist



Subcutaneous tumor



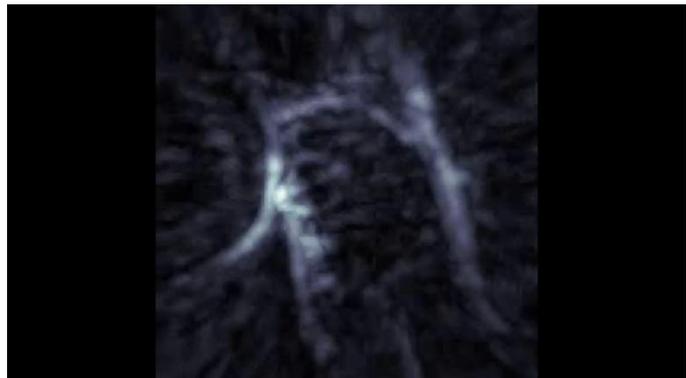
Herzog E. et al, Radiology, 38 (9), 2012

Deán-Ben XL. and Razansky D., Light Sci Appl, 3, 2014

# Photoacoustic imaging : applications for endogenous contrast

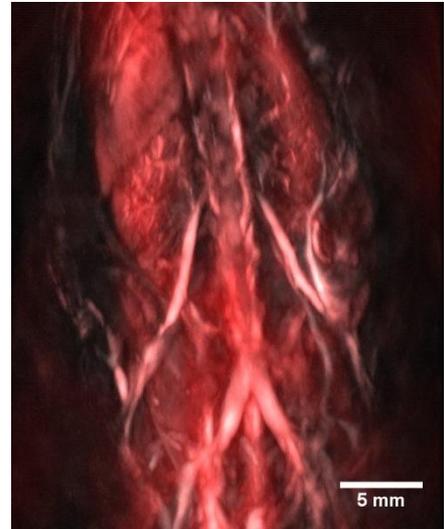
✓ Angiography and perfusion

Human forearm



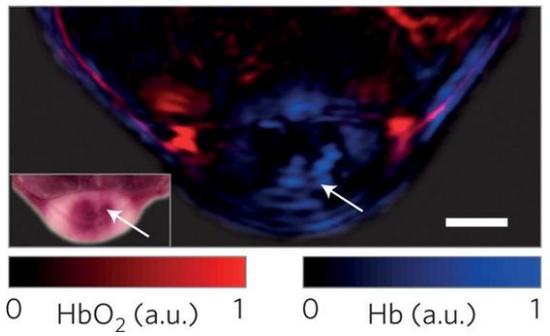
Deán-Ben XL. and Razansky D., Photoacoustics 1 (3-4), 2013

Mouse

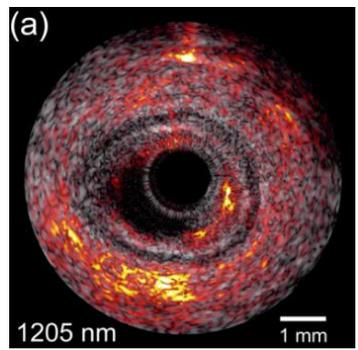


Gateau J. et al, Medical Phys. 40 (1), 2013

✓ Tumor heterogeneity and hypoxia



Herzog E. et al, Radiology, 38 (9), 2012



Jansen K. et al, Opt. Exp., 21 (18), 2013

✓ Atheroma: vulnerable plaques

# Synthesis

	Diffuse optics TR-DOT	Photoacoustics
Image contrast		<b>Absorption</b>
Spatial resolution		< 1 mm ~ penetration depth/200 <i>depending on the number and distribution of detectors</i>
Penetration depth		Max. 4 cm
Temporal resolution		0.01 – 10 images/s <i>depending on the number of detectors</i>
Accessible organs		All externally or endoscopy except brain (adults) and lungs
Typical contrast agents		<b>Methylene blue, Indocyanine green, Gold nanoparticles</b>

# Conclusion

Both diffuse optical imaging and photoacoustic imaging techniques :

- are **non-invasive** and **non-ionizing**
- can reveal **endogenous contrast** with anatomical and functional information **at cm-depth** in tissue *in vivo*
- report results in **real-time** (depending on the set-up).
- may be **bedside** and allow **longitudinal** studies.
- **Applications** : mapping blood oxygenation, tumor, hemorrhage, vulnerable plaque ... + *molecular contrast agents*.
- are complementary:
  - **Photoacoustics**: spatial resolution and depth
  - **Diffuse optics**: scattering and monitoring ability

# Comparison of the methods

	Diffuse optics TR-DOT	Photoacoustics
Image contrast	Absorption and scattering	Absorption
Spatial resolution	From ~ mm at surface to ~ cm in depth <i>depending on the number of source/detector pairs, depth and (<math>\mu_a, \mu_s'</math>)</i>	< 1 mm ~ penetration depth/200 <i>depending on the number and distribution of detectors</i>
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Typical contrast agents	Indocyanine green	Methylene blue, Indocyanine green, Gold nanoparticles